

Low-intensity vibrations normalize adipogenesis-induced morphological and molecular changes of adult mesenchymal stem cells

Proc IMechE Part H:
J Engineering in Medicine
2017, Vol. 231(2) 160–168
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DOI: 10.1177/0954411916687338
journals.sagepub.com/home/pih


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Abstract

Bone marrow mesenchymal stem cells that are committed to adipogenesis were exposed daily to high-frequency low-intensity mechanical vibrations to understand molecular, morphological and ultrastructural adaptations to mechanical signals during adipogenesis. D1-ORL-UVA mouse bone marrow mesenchymal stem cells were cultured with either growth or adipogenic medium for 1 week. Low-intensity vibration signals (15 min/day, 90 Hz, 0.1 g) were applied to one group of adipogenic cells, while the other adipogenic group served as a sham control. Cellular viability, lipid accumulation, ultrastructure and morphology were determined with MTT, Oil-Red-O staining, phalloidin staining and atomic force microscopy. Semiquantitative reverse transcription polymerase chain reaction showed expression profile of the genes responsible for adipogenesis and ultrastructure of cells. Low-intensity vibration signals increased viability of the cells in adipogenic culture that was reduced significantly compared to quiescent controls. Low-intensity vibration signals also normalized the effects of adipogenic condition on cell morphology, including area, perimeter, circularization and actin cytoskeleton. Furthermore, low-intensity vibration signals reduced the expression of some adipogenic markers significantly. Mesenchymal stem cells are sensitive and responsive to mechanical loads, but debilitating conditions such as aging or obesity may steer mesenchymal stem cells toward adipogenesis. Here, daily application of low-intensity vibration signals partially neutralized the effects of adipogenic induction on mesenchymal stem cells, suggesting that these signals may provide an alternative and/or complementary option to reduce fat deposition.

Keywords

Mesenchymal stem cells, vibrations, *in vitro* cell culture, mechanical signals, adipogenic commitment, bone marrow

Date received: 13 November 2015; accepted: 9 December 2016

Introduction

Obesity is a multifactorial disease that leads to serious health problems such as type 2 diabetes, cardiovascular and cerebrovascular diseases, hypertension, digestive disorders and cancer. The number of deaths declared by the World Health Report shows the severity of the problem which indicates that more than 2.5 million of deaths worldwide per year are weight related.¹ Increased fat content in adipose tissue is the hallmark of obesity² and that increase is related to genetic factors³ as well as poor diet⁴ and sedentary lifestyles.⁵ Even though fat accumulation occurs mainly in subcutaneous and visceral adipose tissues,⁶ bone marrow space is also affected and filled with adipocytes during obesity.⁷

The bone marrow fat is originated from adult mesenchymal stem cells,⁸ and even progenitor cells that are committed to bone formation have the capability to

form marrow adipocytes.⁹ Studies show that obesity inducing factors, such as high fat diet^{10,11} or leptin deficiency,¹² may disturb bone marrow mesenchymal stem cell population, increase bone marrow fat and be detrimental to bone structure. These observations are supported by clinical evidence that an inverse relationship exists between bone marrow fat and bone mass.^{13–15} Bone marrow fat may be a serious threat to bone

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health, not only because adipocytes compete with the osteoblasts for the same stem cell pool, but also the bone marrow composition can become more adipogenic and pro-inflammatory during the progression of fat accumulation.¹⁶ Protection of bone marrow from adipogenesis may require strategies that directly affect stem cell population and steer commitment of those cells to osteogenesis from adipogenesis.¹⁷ Out of those strategies, efforts of daily mechanical intervention showed promising results in suppressing marrow adipogenesis during diet-induced obesity in mice.⁷ Suppressing marrow adipogenesis with a non-pharmaceutical strategy that also affects other organs and systems positively is plausible, yet the information on which constituents of a mechanical signal is sensed and responded by bone marrow stem cells is still limited.^{18,19}

Bone cells sense and respond to different forms of mechanical loads, including cyclic stretch,²⁰ static pressure,²¹ shear stress^{22,23} and nanoscale mechanotransduction.^{24,25} In addition to these loading variants, daily application of low-intensity (< 0.5 g, 1 g = 9.81 m/s²) vibrations (LIVs) in high frequencies (> 30 Hz) is anabolic to bone tissue and can suppress obesity in murine and clinical studies.^{26–28} LIV can also help maintaining a healthy bone marrow during conditions that are detrimental to bone marrow, such as mechanical disuse²⁹ or diet-induced obesity.³⁰ On cellular level, LIV acts as pro-osteogenic to bone marrow stem cells and influences their proliferation, morphology, cell-to-cell communication and molecular markers *in vitro*^{31–33} but cells of other developmental origins, such as epithelial cells, appear to be less sensitive to LIV signals.³⁴ Furthermore, *in vitro* application of LIV signals during adipogenesis inhibit lipid accumulation.³⁵

Application of LIV *in vitro* induces a broad range of cellular and molecular responses to osteoprogenitor cells,^{36,37} however these responses are less known for stem cells that are committed to adipogenesis. Here, we subjected D1-ORL-UVA mouse bone marrow stem cells daily to LIV signals during induced adipogenesis to document isolated cellular adaptation of stem cells on morphological, ultrastructural and molecular level.

Materials and methods

Cell culture

Mouse bone marrow pluripotent stem cell line D1-ORL-UVA (American Type Culture Collection, USA) that is able to differentiate into all mesenchymal cell types including adipocytes was used in all experiments. D1-ORL-UVA cells were grown and maintained in Dulbecco's Modified Eagles Medium (DMEM; Thermo Scientific HyClone, USA) supplemented with 10% fetal bovine serum (Biological Industries, Israel) and 1% penicillin/streptomycin (Biological Industries, Israel) as instructed by the

vendor. For all experiments, D1-ORL-UVA cells were used between passages 6 and 12. Adipogenic induction is achieved by addition of 5 μ g/mL of insulin (Sigma, USA), 50 μ M of indomethacin (Sigma, USA) and 10 nM of dexamethasone (Sigma, USA) to the growth medium, which can induce lipid accumulation. For all experiments except atomic force microscopy (AFM) and reverse transcription polymerase chain reaction (RT-PCR), D1-ORL-UVA cells were plated at a density of 500 cells/well in 24-well plates (Corning, USA) for individual cell morphology analysis and maintained in the growth medium at 37°C and 5% CO₂. Plated cell number was selected based on the criteria that at the end of experiment, cells would reach to 80%–90% confluency. For AFM experiments, 8×10^4 cells were grown on 10 cm plates and 5×10^3 cells were grown on 6-well plates for RT-PCR experiments. During experiments, cells were first allowed to adhere to the culture plate for 2 days and then media was either refreshed (for quiescence) or changed with adipogenic media (for adipogenesis). Culture media was changed every 3 days and all experiments were terminated at day 9 for morphology, lipid content, mRNA expressions and AFM. Some cultures were continued to assess osteogenic potential of D1-ORL-UVA cells after adipogenic induction. For those experiments, osteogenic supplements (1000 μ g/mL ascorbic acid and 10 mM β -glycerol phosphate; Sigma, USA) were used to replace adipogenic supplements. These follow-up experiments were either continued for 1 week for mRNA expression or 2 weeks for micrographs of lipid and calcium phosphate accumulation.

Mechanical stimulation

Cells were either subjected to 90 Hz, 0.15 g vibrations for 7 days (15 min/day) under room conditions or received sham treatment to eliminate the effects of ambient conditions.^{31,34} Briefly, proper sinusoidal signals were generated via a custom-made platform (Figure 1) and the brevity of this mechanical signal was continuously monitored with a real-time accelerometer (K-Beam; Kistler, USA) through LabVIEW 2010 Signal Express software (National Instruments, USA). D1-ORL-UVA cells that were kept in the growth media and received daily sham loading were reported as Growth Control (GC). D1-ORL-UVA cells that were cultured in adipogenic media that received daily loading were reported as Adipogenic Vibration (AV), while adipogenic D1-ORL-UVA cells that received sham loading were reported as Adipogenic Control (AC). To understand long-term osteogenic potential, after 9 days, GC, AC and AV groups were continuously cultured in osteogenic media (GCO—Growth Control followed by osteogenic induction, ACO—Adipogenic Control followed by osteogenic induction and AVO—Adipogenic Vibration followed by osteogenic induction).

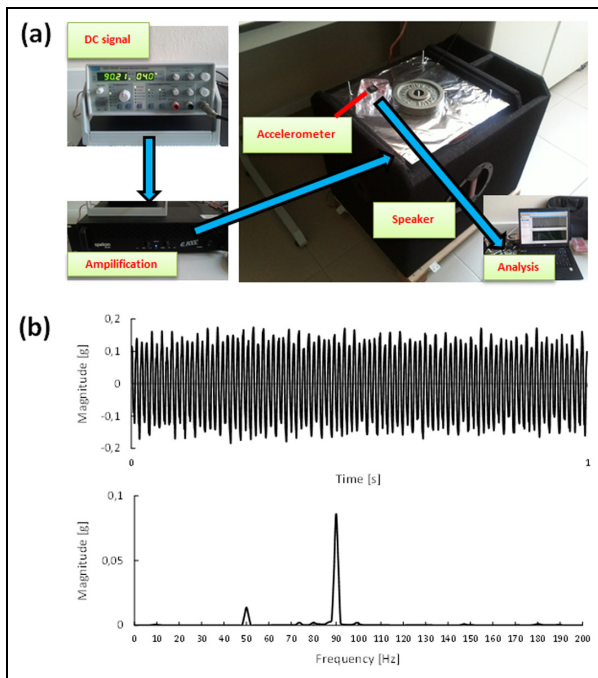


Figure 1. Mechanical stimulation applied to the cells at 90 Hz and 0.15 g for the study: (a) components of the mechanical vibration delivery platform and (b) representative data from time and frequency domains. Note that the small peak in 50 Hz corresponds to the electromagnetic noise from the power grid.

Cell growth and viability

At day 9, cell viability was analyzed via MTT (3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide) assay, in which cells were incubated with 0.5 mg/mL MTT (AMRESCO LLC, USA) for 4 h. After the incubation, tetrazolium salts were dissolved in 600 μ L dimethyl sulfoxide (DMSO) for 2 min and colorimetric measurements were done at 570 nm with a background subtraction at 650 nm.

Immunostaining and fluorescent microscopy

Cells were washed with phosphate buffered saline (PBS) and fixed with 4% paraformaldehyde (PFA) for 20 min. PFA was triple washed with PBS followed by membrane permeabilization with 0.1% Triton X/PBS for 15 min. Cells were blocked with 3% bovine serum albumin (BSA) in 0.1% Triton X/PBS for 30 min and were then incubated with Alexa488-conjugated phalloidin (Invitrogen, USA) for 30 min in the dark for the imaging of actin filaments. After gentle washing with PBS, cells were incubated in 4',6-diamidino-2-phenylindole (DAPI) solution for visualization of nuclei. Images were acquired with an inverted microscope and fluorescent attachment (CKX71; Olympus, Japan). A minimum of 10 sample images were used for signal intensity measurement per condition from three different experiments. Images were analyzed using ImageJ software. Lipid content of cells was determined with Oil-Red-O

staining, while calcium phosphate accumulation was determined with alizarin red stains.

AFM

Nanosurf FlexAFM (Nanosurf, Switzerland) was used to get AFM images. Cells were probed with Non-Contact/Tapping Mode-Long Cantilever-Reflex Coating (NCLR) tip with 190 kHz resonance frequency and 48 N/m force constant in DMEM. Scans were conducted with 71.4143 kHz vibration frequency and 3.07 mV vibration amplitude. Cells were analyzed for average surface roughness (R_a), root-mean-square roughness (R_q), maximum height (R_y), maximum peak height (R_p) and maximum valley depth (R_v) using AFM image processing software Nanosurf Scan.

Gene expression analysis

Cells were lysed and total mRNA was isolated using PureLink RNA mini kit (Invitrogen, USA). After verification of purity and determination of concentration with NanoDrop (ND-1000; Thermo Scientific, USA), two-step real-time PCR was performed. For reverse transcription reaction, RevertAid first strand cDNA synthesis kit (Thermo Scientific, USA) was used with 1000 ng template RNA. cDNA samples of 7.5 μ L were loaded with 12 μ L of Sybr Green (Thermo Scientific, USA), 2.5 μ L forward and reverse primers of adipogenic, osteogenic markers and cytoskeletal molecules for semiquantitative RT-PCR (Bio-Rad, USA), where GAPDH (glyceraldehyde 3-phosphate dehydrogenase) was used as the house-keeping molecule (Table 1). For all groups, 3–4 samples were used for gene expression analysis.

Statistical analysis

All results were expressed as mean (\pm standard deviation). Group comparisons were done using unpaired t-tests between growth and adipogenic as well as control and vibration groups, in which the threshold for statistical significance was set to 5%.

Results

Adipogenic induction and cell viability

Adipogenic induction resulted in positive Oil-Red-O signal showing the lipid accumulation in D1-ORL-UVA cells at the end of first week, while stem cells that remained in growth media did not show any signal (Figure 2(a) and (b)). Cells that received mechanical vibrations showed lipid accumulation to a lesser extent (Figure 2(c)). Viability of AC cells was 28% ($p < 0.01$) smaller compared to GC cells. Daily application of LIV signal increased observed viability in AV group by 45% ($p < 0.01$) compared to AC cells (Figure 3).

Table 1. Primers designed for the gene expression analysis of cytoskeletal elements, adipogenic and osteogenic markers for D1-ORL-UVA mouse mesenchymal stem cells. GAPDH (glyceraldehyde 3-phosphate dehydrogenase) was used as the house-keeping molecule for all groups.

Gene	Direction	Sequence
β-Actin	F	CTT CTT TGC AGC TCC TTC GTT
	R	TTC TGA CCC ATT CCC ACC A
Desmin	F	GTG AAG ATG GCC TTG GAT GT
	R	GTA GCC TCG CTG ACA ACC TC
Vimentin	F	ACG GTT GAG ACC AGA GAT GG
	R	CGT CTT TTG GGG TGT CAG TT
Lamin	F	ATC AAC TCC ACT GGA GAA GAA GT
	R	CAG ACA GGA GGT GGC ATG T
Collagen Ia	F	CAC CCT CAA GAG CCT GAG TC
	R	AGA CCG CTG AGT AGG GAA CA
β-catenin	F	AAG GAA GCT TCC AGA CAT GC
	R	GCT TGC TCT CTT GAT TGC C
Osteocalcin	F	CTG ACA AAG CCT TCA TGT CCA A
	R	GCG CCG GAG TCT GTT CAC TA
Adipsin	F	GCT ATC CCA GAA TGC CTC GTT
	R	CCA CTT CTT TGT CCT CGT ATT GC
Resistin	F	CAA CTC CCT GTT TCC AAA TGC
	R	CTC AAG ACT GCT GTG CCT TCT
C/EBP-α	F	TGG ACA AGA ACA GCA ACG AGT AC
	R	GCA GTT GCC CAT GGC CTT GAC
ENC-1	F	AAG CTT CCG CAT A
	R	AAG CT ₁₁ A
PPAR _γ	F	GCC TTG CTG TGG GGA TGT C
	R	TCCTTGGCCCTCTGAGATGAG
PTK2	F	TTG GAC CTG GCA TCT TTG AT
	R	AGA ACA TTC CGA GCA GCA AT
GAPDH	F	GAC ATG CCG CCT GGA GAA AC
	R	AGC CCA GGA TGC CCT TTA GT

Cell morphology and AFM

Morphological and ultrastructural differences induced by adipogenesis and daily application of LIV were quantified by single-cell analysis. Adipogenic induction reduced cellular area by 39% ($p < 0.01$) compared to GC cells (Figure 4(a)). LIV-applied AV cells showed 18% ($p = 0.05$) larger area compared to AC cells. Similarly, cellular perimeter was reduced by 42% ($p < 0.01$) in AC group compared to GC group but vibrations increased AV cell perimeter by 20% ($p < 0.01$) compared to AC group (Figure 4(b)). Adipogenic conditions also increased the circularity of AC cells by 50% ($p < 0.01$) compared to GC group (Figure 4(c)). AV group had a 20% ($p < 0.01$) decrease in circularity compared to AC cells. Actin fluorescent signal per area was increased twofold ($p < 0.01$) with adipogenic induction (Figure 4(d)). Mechanical vibrations reduced the actin signal in AV group 22% ($p < 0.01$) compared to AC cells.

Membrane probing for all groups using fluid-cell AFM showed that adipogenic induction reduced average membrane roughness of AC cells by 60% ($p < 0.05$) but vibrations did not induce any change ($p = 0.4$) in average roughness (Figure 5). Similarly, application of LIV signals did not change the R_q , R_y of cell surface, R_v of the cell surface roughness and R_p (Table 2).

Gene expression

Molecular changes in bone marrow stem cells during adipogenesis and vibrations were analyzed by semi-quantitative RT-PCR (Figure 6). Results showed that neither adipogenesis nor vibration change the expression of ultrastructural molecule actin, desmin and lamin as well as β-catenin levels in D1-ORL-UVA cells. Vimentin level was decreased by 36% ($p < 0.05$) in AV group compared to AC cells. Adipogenic induction reduced the collagen level by 60% ($p < 0.05$) compared to GC cells and AV cells showed a decline by 57% ($p < 0.01$) relative to AC cells. Adipogenic markers adipsin and resistin were increased in AC cells by 19-fold and 214-fold (both $p < 0.05$), while vibration decreased the expression level of these genes by 59% and 94%, respectively (both $p < 0.05$). Another adipogenic marker c-EBPα was increased by 55% ($p = 0.05$) in AC cells compared to GC cells, and its expression was normalized with vibration by 52% ($p < 0.05$) in AV group. PPAR_γ which is another regulator of adipogenesis showed a 40% ($p < 0.05$) decrease in AV cells compared to AC cells. Moreover, expression level of ENC-1 gene was normalized and showed a closer level with GC cells via vibration by 2.5-fold increase in AV group compared to AC group ($p = 0.01$).

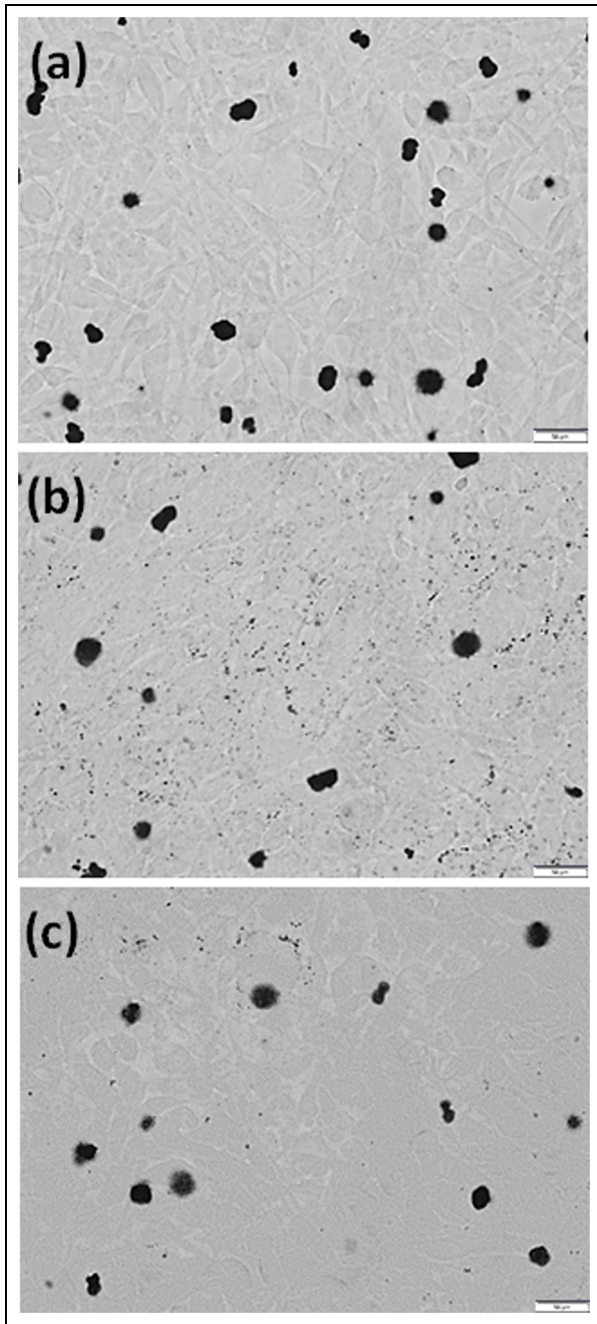


Figure 2. Light microscopy of Oil-Red-O stain (lipid accumulation) in D1-ORL-UVA cells after 1 week of culture in (a) growth media, (b) adipogenic media and (c) adipogenic media with daily application of mechanical vibrations.

Osteogenic potential

To test multipotency of D1-ORL-UVA cells after adipogenic induction, we replaced adipogenic supplements in the media with osteogenic supplements. Cells that did not receive adipogenic supplement earlier (GCO) were able to form clear mineral deposition after 2 weeks of osteogenic culture (Figure 7(a)). Adipogenic culture cells (ACO) were also able to form mineral deposits to a lesser extent once exposed to osteogenic conditions. Cells that received LIV during adipogenesis (AVO) showed larger accumulation of deposits during

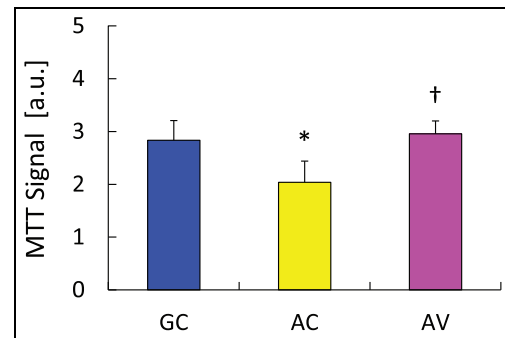


Figure 3. Viability of the cells as quantified by MTT assay. GC: Growth Control; AC: Adipogenic Control; AV: Adipogenic Vibration.

Results are presented as mean \pm SD.

* $p < 0.05$ between GC and AC; † $p < 0.05$ between AC and AV.

osteogenesis, even though LIV was discontinued on these cells during osteogenesis (Figure 7(a) and (c)). Furthermore, ACO cells still retained their lipid droplets after 2 weeks unlike AVO cells (Figure 7(c)). Osteocalcin, a molecular marker for osteogenesis was 65% ($p = 0.02$) larger in AVO cells compared to ACO (Figure 7(b)). PPAR γ of AVO cells on the other hand showed a trend (-40% , $p = 0.15$) in being smaller compared to ACO cells.

Discussion

Morphological and molecular effects of LIV on bone marrow mesenchymal stem cells during adipogenic commitment were investigated in this study. LIV signal was applied daily for 15 min/day in low magnitude (0.15 g) and high frequency (90 Hz) for 1 week. Results showed that adipogenesis-induced changes in morphological and molecular markers of stem cells were partially normalized with daily mechanical signals similar to quiescent controls. LIV application helped stem cells to retain their osteogenic potential better once the adipogenic environment was removed.

Inhibition of adipogenesis using mechanical signals *in vitro* was initially studied using low-frequency, high-magnitude signals, similar to those that are experienced during strenuous exercise. It was shown that application of cyclic mechanical stretching² and uniform biaxial strain³⁸ reduced lipid accumulation in fibroblasts. Reduced lipid accumulation in fibroblasts was linked to the increased expression of β -catenin³⁵ and suppression in PPAR γ .² Observations on the suppressive effect of mechanical signals were also held with lower magnitude and higher frequency signal form, both *in vivo*^{26,27,39} and *in vitro*.^{2,38,40} Although our results did not indicate a drastic change in β -catenin levels and possible involvement of WNT pathway in D1-ORL-UVA cells, we observed that expression levels of various adipogenic markers were significantly reduced with the presence of LIV signals. Adipsin,⁴¹ c/EBP- α ⁴² and PPAR γ ^{43,44} are important adipocyte specific markers and significant

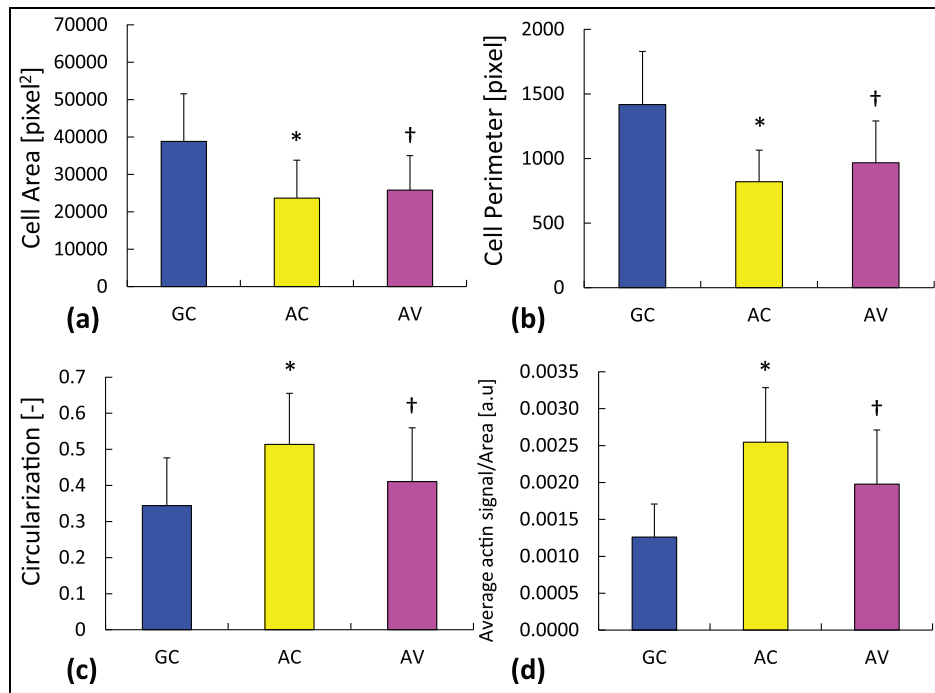


Figure 4. Differences in morphological and ultrastructural properties of cells including (a) area, (b) perimeter, (c) circularization and (d) area normalized actin signal.

GC: Growth Control; AC: Adipogenic Control; AV: Adipogenic Vibration.

Results are presented as mean \pm SD.

* $p < 0.05$ between GC and AC; † $p < 0.05$ between AC and AV.

Table 2. Components of cellular membrane roughness recorded with AFM probing including root-mean-square roughness (Rq), maximum height (Ry) of cell surface, maximum valley depth (Rv) of the cell surface roughness and maximum peak height (Rp).

Group	Rq (nm)	Ry (nm)	Rv (nm)	Rp (nm)
GC	2.86 \pm 1.46	13.97 \pm 5.74*	-3.22 \pm 2.17	10.75 \pm 3.62*
AC	0.65 \pm 0.26	3.71 \pm 1.34*	-1.73 \pm 1.10	1.99 \pm 0.30*
AV	0.59 \pm 0.07	3.18 \pm 0.77	-1.47 \pm 0.31	1.71 \pm 0.59

GC: Growth Control; AC: Adipogenic Control; AV: Adipogenic Vibration; SD: standard deviation; Rq: root-mean-square roughness; Ry: maximum height; Rv: maximum valley depth; Rp: maximum peak height.

Results are presented as mean \pm SD.

* $p < 0.05$ between Growth Control and Adipogenic Control groups.

suppression in their expression suggests that LIV suppresses adipogenic commitment and differentiation of bone marrow stem cells.

Application of LIV signals during adipogenic induction also resulted in physical changes in the bone marrow stem cells. Adipogenesis-induced circularization in bone marrow stem cells⁴⁴ was suppressed with LIV signals. Actin network is the main determinant of the shape and structure of cells, and actin remodeling is required for adipogenesis.⁴⁵ The rearrangement and increase in actin provide stability to the cell shape during lipid accumulation.^{45,46} Our previous results showed that LIV application increased total actin content in bone marrow stem cells during quiescence and osteogenic commitment but that increase was homogeneous through the cell.³¹ Here, actin signal for adipogenic cells was mainly observed in cellular periphery but actin signal was lower when the circularization was

reduced and fibroblastic shape retained. In addition to actin, ENC-1, an actin binding protein, plays mediatory role in differentiation of fibroblastic preadipocytes to mature adipocytes during cytoskeletal reorganization and consistent with our results, its expression levels are scant in mature adipocytes,⁴⁷ suggesting that stem cells in AC group reached to maturity faster *in vitro*, while LIV-applied cells were either delayed or reverted to quiescent like characteristics.

In addition to shape and motility, cellular ultrastructure also determines the mechanical properties and stiffness of cells.^{48,49} Bone marrow stem cells decrease their global mechanical stiffness during adipogenesis,⁴⁹ possibly reflecting that reorganization of actin filaments in the cellular periphery is not supported with cortical stress fibers. Our results suggested that despite the increase in peripheral actin signal, cellular cortex was smoother as measured via AFM indicating that

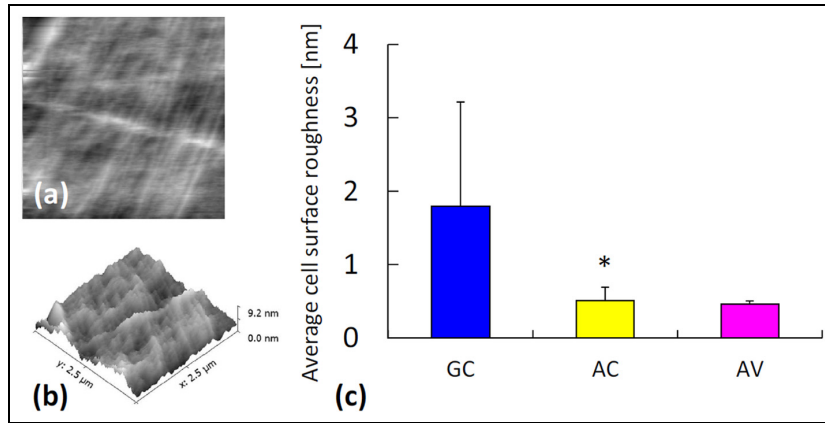


Figure 5. Membrane probing of DI-ORL-UVA cells in culture media using AFM: (a) representative surface map, (b) 3D surface and (c) average cellular membrane roughness.

GC: Growth Control; AC: Adipogenic Control; AV: Adipogenic Vibration.

Results are presented as mean ± SD.

*p < 0.05 between GC and AC.

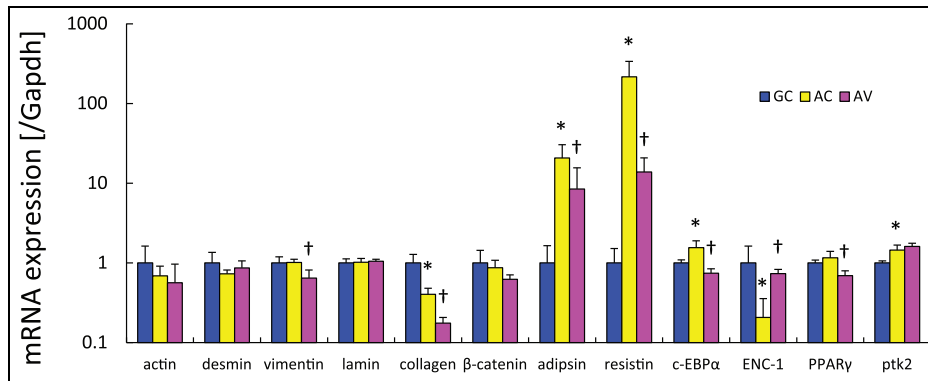


Figure 6. Molecular expression of selected cytoskeletal or adipogenic markers measured by qPCR normalized to house-keeping gene (GAPDH).

GC: Growth Control, AC: Adipogenic Control, AV: Adipogenic Vibration.

Results are presented as mean ± SD.

*p < 0.05 between GC and AC; †p < 0.05 between AC and AV.

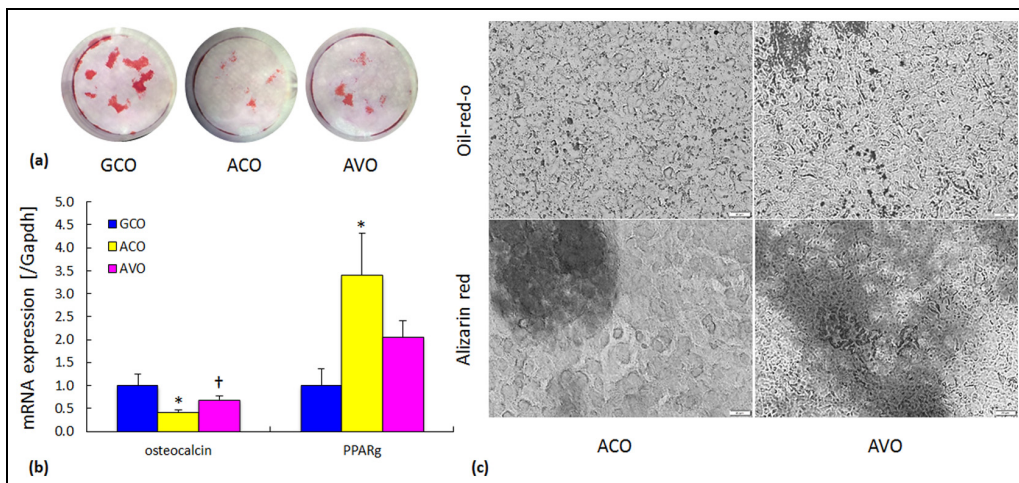


Figure 7. Osteogenic potential of DI-ORL-UVA cells after 1 week of adipogenic induction: (a) global alizarin red staining,

(b) molecular expression of osteocalcin and PPARγ and (c) micrographs from alizarin red and Oil-Red-O stains.

GCO: Growth Control followed by osteogenic induction; ACO: Adipogenic Control followed by osteogenic induction with no adipogenic induction;

AVO: Adipogenic Vibration followed by osteogenic induction with no adipogenic induction and vibration.

Results are presented as mean ± SD.

*p < 0.05 between GCO and ACO; †p < 0.05 between ACO and AVO.

LIV signals did not induce any change in cortex roughness. Since cells may lose their thicker actin fibers during adipogenic differentiation and form new fibers oriented in a thinner conformation after differentiation,⁵⁰ perhaps, the resolution of AFM was not able to probe these thin filaments.

Cytoskeletal elements are also important modulators of cellular mechanosensitivity, linking regional or global deformations elsewhere in the cell to nuclear processes.^{51,52} Bone marrow mesenchymal stem cells are readily sensitive and responsive to mechanical loads, however pathological conditions such as aging and obesity reduce their mechanosensitivity and therefore bone marrow adipogenesis increases with a reduction in bone mass.¹⁸ These phenomena are corroborated with degradations in cytoskeletal assembly during aging and adipogenesis,^{53,54} suggesting that bone marrow stem cells may not be able to benefit from LIV signals with high efficacy. Restoration of mechanosensitivity during debilitating conditions may be required to revert and increase osteogenic potential of adipocyte committed mesenchymal stem cells. Improved understanding on the sub-cellular determinants of mechanosensitivity may guide the clinical efforts for the suppression of bone marrow adipogenesis and increase in bone mass during aging and obesity.

Acknowledgements

The author(s) thank Melis Olcum, Hadi M Zareie, Ozden Yalcin-Ozuysal and Biotechnology and Bioengineering Research and Application Center, Izmir Institute of Technology for expert technical help.

Declaration of conflicting interests

The author(s) declared no potential conflicts of interest with respect to the research, authorship and/or publication of this article.

Funding

The author(s) disclosed receipt of the following financial support for the research, authorship, and/or publication of this article: This work was funded by the Scientific and Technological Research Council of Turkey (111T577).

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